Biofluid Simulation and Modeling Lichtenberg Junior Research Group





ESPResSo for blood flow

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Blood flow



I. Immersed-boundary



Red blood cell in a microchannel



Blood flow with drug delivery agents



Immersed boundary

Lattice-Boltzmann D3Q19

• Implemented in ESPResSo



Immersed-Boundary for cells

- Implemented in developer version of ESPResSo
- Python interface almost finished
- Requires
 - Computation of elastic forces
 - Two-way coupling between cell membrane and fluid



Red blood cell model

- Typical discretization
 - 1280 triangles
 - 642 nodes



Red blood cell model

- Shear & stretch
 - Skalak model
 - phenomenological energy density

$$W = \frac{\kappa_{s}}{4} \left(\frac{1}{2} I_{1}^{2} + I_{1} - I_{2} \frac{1}{2} + \frac{\kappa_{a}}{8} I_{2}^{2} \right)$$

- shear modulus
- area conservation modulus
- parameters from experiments, e.g. optical stretching, micropipette aspiration
- forces on nodes by taking derivatives (Hamilton formalism)



RBC model

- Bending resistance
 - Helffirthmodel

$$E_{\rm B} = \int_{S} 2\kappa_{\rm B} \left(H - H_0\right)^2 \mathrm{d}S$$

- bending modulus κ_B

- curvature

$$H(\boldsymbol{x}) = \frac{1}{2} \sum_{i=1}^{3} \left(\Delta_{\mathrm{S}} x_i \right) n_i(\boldsymbol{x})$$

- bending force density

 $\Delta \boldsymbol{f}_{\mathrm{B}} = -2\kappa_{\mathrm{B}} \underbrace{\Delta_{\mathrm{S}} (H - H_{0})}_{+ 2 (H - H_{0}) (H^{2} - K + H_{0}H)] \boldsymbol{n}$



RBC model

- Bending algorithms
 - Three classes:
 - weak, strong, force formulation
 - Guckenberger and Gekle J. Phys. Cond. Mat. 2017
 - Comparison of five methods





Guckenberger, Schraml, Chen, Leonetti and Gekle Comput. Phys. Commun. 2016



Coupling to fluid: immersed boundary

- Membrane nodes are off-lattice
- Forces into fluid
 - force on each node acts as source term to Navier-Stokes equations
 - forces are distributed to surrounding LBM nodes
- Membrane node advection
 - interpolate velocity from surrounding LBM nodes
 - IBM nodes follow the fluid exactly
- Membrane nodes have no mass
 - enforces strictly no-slip
 - thermodynamically they are not independent degrees of freedom



Implementation in ESPResSo

- Membrane nodes are *virtual* particles
- They are ignored by the Verlet loop
- Skalak and Helfrich bending as new interactions
- Additional interaction for volume conservation
- Works with GPU and CPU LBM
- Current bottleneck for GPU:
 - Forces and LB fluid cannot be computed in parallel

I. A single red blood cell

Setup

- A single red blood cell in a cylindrical microchannel
- Lattice-Boltzmann immersed boundary
- Flow driven by body force in LBM
- or by poor man's inflow boundary conditions

Modes of motion

- Discocyte
- Parachute
- Croissant
- Slipper
- Tumbling









Fig. 2: Without temperature. Cells started rotated and in the center.

Model validation

(a) 3D measurements







slipper perspective

slipper side

croissant perspective

croissant side

Quint, Christ, Guckenberger, Himbert, Kästner, Gekle, Wagner Appl. Phys. Lett. 2017 Guckenberger, Kihm, John, Wagner, Gekle in preparation III. Margination at constrictions

Straight channel



 $R_{c} = 13.4 \ \mu m$ $R_{p} = 1.6 \ \mu m$ 52 RBCs Ht = 19%
4 particles $V_{max} = 2.5 \text{mm/s}$

Straight channel

x [µm]



x [µm]

Constriction



 $R_{c} = 13.4 \ \mu m$ $R_{constr}/R_{c} = 1/2$ 108 RBCs Ht = 16%
18 particles $V_{max} = 1 mm/s$

Constriction



Radially averaged profile: RBCs



Radially averaged profile: RBCs





Radially averaged profile: RBCs





Radially averaged profile: microparticles





Radially averaged profile: suspension



Bächer, Schrack and Gekle Phys. Rev. Fluids (2017)

Radially averaged profile: suspension



Clustering mechanism



Microparticles squeeze into RBC layer

Clustering is robust



Phys. Rev. Fluids (2017)

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Computing power







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